

# Sparsity Through Annihilation

## Algorithms and Applications

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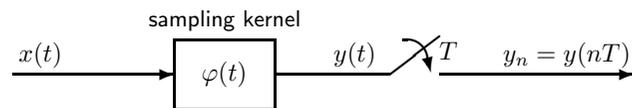
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## Outline

- 1 Signal Interpolation
- 2 Annihilation algorithms
- 3 Noisy annihilation
- 4 Application: Optical Coherence Tomography
- 5 Conclusion

## A very old problem

Given a sampling device that provides smooth, *uniform* samples  $y_n$  of a "real-world" function  $x(t)$



How to reconstruct  $x(t)$  *exactly*, and under which conditions?

**NOTE:** Implicitly, there is the assumption that if the samples are *shifted*, then the reconstruction should also be shifted by the *same amount*.

Observation kernel  $\varphi(t)$ : often given partly by nature, partly by design.

Hubble telescope



Electro-EncephaloGraphy



OCT Set-Up



MRI scanner



### Standard solution (from Shannon, Whittaker, Kotel'nikov, Nyquist, ...)

If  $x(t)$  is *band-limited* in  $]-\pi/T, \pi/T[$  and  $\hat{\varphi}(\omega) \neq 0$  in that band, then the knowledge of its samples  $y_n$  at the frequency  $1/T$  allows to reconstruct  $x(t)$  *uniquely* by

$$x(t) = \sum_{n \in \mathbb{Z}} y(nT) \psi(t - nT)$$

where  $(\varphi * \psi)(t) = \text{sinc}(t/T)$ .

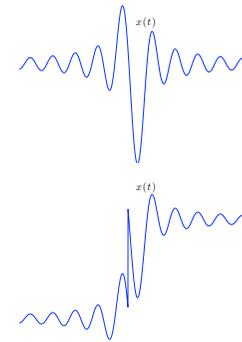
**Problems**  $\leadsto$  need for a better adapted signal model

- the samples are almost always in *finite* number
- a natural signal is *never* band-limited
- noise sensitivity of Shannon's formula

**NOTE:** Replacing sinc by other "basis" functions (e.g., splines) addresses these issues, but fails to produce *shift-invariant* solutions.

### Shannon's nightmare

An *ideal band-limited* signal  $x(t)$  can be represented exactly by its samples  $x(nT)$



But a *single discontinuity* and no more sampling theorem.

**NOTE:** Bandlimited signals are represented using  $1/T$  degrees of freedom per unit of time.

Are there other shift invariant signal families with finite numbers of degrees of freedom per unit of time, and allowing perfect reconstruction?

## Signals with Finite Rate of Innovation

A novel signal model, that emphasizes the *duality* of the "information" —the *innovation*— conveyed by a signal

- A *linear* aspect : e.g., the amplitude of a sample
- A *nonlinear* aspect: e.g., a time of change of the signal

The FRI hypothesis<sup>1</sup> 

A Finite Rate of Innovation signal can be expressed as the convolution of an acquisition window with a stream of Diracs

$$y(t) = \left( \sum_{k=-\infty}^{+\infty} x_k \delta(t - t_k) \right) * \varphi(t) = \sum_{k=-\infty}^{+\infty} x_k \varphi(t - t_k)$$

$x_k$  and  $t_k$  are called the *innovations* of the signal.

*Rate of innovation:* the average number of innovations per unit of time.

<sup>1</sup>M. Vetterli, P. Marziliano, and T. Blu, "Sampling signals with finite rate of innovation," *IEEE Trans. on Signal Processing*, vol. 50, pp. 1417–1428, June 2002.

### Examples

- Piecewise-constant signals

- OCT signals: convolution with a Gabor window



- ... and many more "sparse" signals

Are there interpolation formulas for such signals?

## Annihilation of periodic signals

Consider the case

- $\tau$ -periodic signal  $x(t) = x(t + \tau)$ , where  $\tau = NT$ ,  $N$  integer
- $\varphi(t) = \text{sinc}(Bt)$  with  $BT = \frac{2M+1}{N} \leq 1$ ,  $M$  integer
- rate of innovation,  $2K/\tau \leq B$  ( $K =$  number of Diracs in  $[0, \tau]$ )

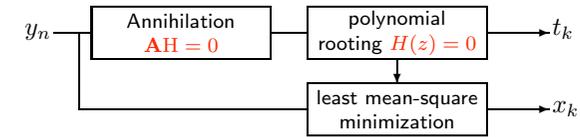
Then the filter of transfer function  $H(z) = \prod_{k=1}^K (1 - e^{-j2\pi \frac{t_k}{\tau}} z^{-1})$  annihilates the  $N$ -DFT coefficients of  $y_n$

$$\sum_{k=0}^K h_k \hat{y}_{m-k} = 0, \quad m = -M + K, \dots, M$$

Under algebraic form, the annihilation equation becomes  $\mathbf{A}\mathbf{H} = 0$ , where  $\mathbf{A}$  is a Toeplitz matrix

$$\mathbf{A} = \begin{bmatrix} \hat{y}_{-M+K} & \hat{y}_{-M+K-1} & \cdots & \hat{y}_{-M+1} & \hat{y}_{-M} \\ \hat{y}_{-M+K+1} & \hat{y}_{-M+K} & \cdots & \hat{y}_{-M+2} & \hat{y}_{-M+1} \\ \vdots & \ddots & \ddots & \ddots & \vdots \\ \hat{y}_M & \hat{y}_{M-1} & \cdots & \hat{y}_{M-K+1} & \hat{y}_{M-K} \end{bmatrix}$$

Hence, an exact reconstruction algorithm looks like



A non-iterative solution to a non-linear problem:  
two linear systems to solve + polynomial root extraction

## Other annihilation examples

Consider the Gaussian case

- $\varphi(t) = e^{-t^2/(2\sigma^2)}$
- $K$  Diracs to retrieve from  $N$  samples  $n \in [-N/2, N/2]$

Then the filter of transfer function  $H(z) = \prod_{k=1}^K (1 - e^{\frac{t_k T}{\sigma^2}} z^{-1})$  annihilates the samples  $\tilde{y}_n = e^{(nT/\sigma)^2/2} y_n$

$$\sum_{k=0}^K h_k \tilde{y}_{n-k} = 0, \quad m = -N/2 + K, \dots, N/2$$

Consider the non-periodic sinc case

- $\varphi(t) = \text{sinc}(t/T)$
- $K$  Diracs to retrieve from  $N$  samples  $n \in [-N/2, N/2]$

Then the filter of transfer function  $H(z) = (1 - z^{-1})^K$  annihilates the samples  $\tilde{y}_n = (-1^n)P(n)y_n$  where  $P(n) = \prod_{k=1}^K (n - t_k/T)$

$$\sum_{k=0}^K h_k \tilde{y}_{n-k} = 0, \quad m = -N/2 + K, \dots, N/2$$

Consider kernels that satisfy Strang-Fix conditions of order  $L \geq 2K$

- either  $\{1, t, t^2, \dots, t^{L-1}\} \in \text{span}_n\{\varphi(nT - t)\}$
- or  $\{e^{at}, e^{(a+b)t}, e^{(a+2b)t}, \dots, e^{(a+(L-1)b)t}\} \in \text{span}_n\{\varphi(nT - t)\}$

Then the filter of transfer function  $H(z) = \prod_{k=1}^K (1 - e^{bt_k} z^{-1})$  annihilates modified samples  $\tilde{y}_n$

$$\sum_{k=0}^K h_k \tilde{y}_{n-k} = 0, \quad m = K, K+1, \dots, L$$

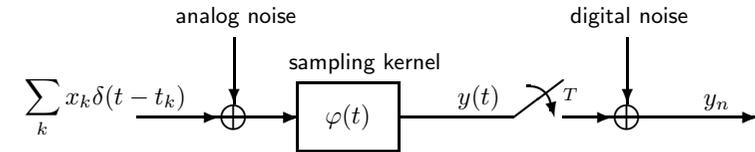
The  $\tilde{y}_n$  are obtained by an adequate linear transformation of the  $y_n$ .

A very large range of observation/analysis kernels (wavelets, etc.)

<sup>1</sup>P.-L. Dragotti, M. Vetterli, and T. Blu, "Sampling moments and reconstructing signals of finite rate of innovation: Shannon meets Strang-Fix," *IEEE Trans. on Signal Processing*, vol. 55, pp. 1741–1757, May 2007.

## FRI with noise

Schematic acquisition of a  $\tau$ -periodic FRI signal with noise



### Modelization

$$y_n = \sum_k x_k \varphi(nT - t_k) + \varepsilon_n$$

## The noisy periodic case

- $\tau$ -periodic signal  $x(t) = x(t + \tau)$ , where  $\tau = NT$ ,  $N$  integer
- $\varphi(t) = \text{sinc}(Bt)$  with  $BT = \frac{2M+1}{N} \leq 1$ ,  $M$  integer
- rate of innovation,  $2K/\tau \leq B$  ( $K$  = number of Diracs in  $[0, \tau]$ )

### Estimation problem

Find estimates  $\tilde{y}_n$ ,  $\tilde{x}_k$  and  $\tilde{t}_k$  of  $y_n$ ,  $x_k$  and  $t_k$  such that

- $\tilde{y}_n = \sum_k \tilde{x}_k \varphi(nT - \tilde{t}_k)$
- $\|\tilde{\mathbf{y}} - \mathbf{y}\|_{\ell^2}$  is as small as possible

## Total least-squares

Replace the annihilation equation  $\mathbf{A}\mathbf{H} = 0$  by

$$\min_{\mathbf{H}} \|\mathbf{A}\mathbf{H}\|^2 \quad \text{under the constraint } \|\mathbf{H}\|^2 = 1$$

### Solution

Perform a *Singular Value Decomposition*

$$\mathbf{A} = \mathbf{U}\mathbf{S}\mathbf{V}^T$$

and choose the **last column** of  $\mathbf{V}$  for  $\mathbf{H}$ .

- $\mathbf{U}$  is *unitary* of same size as  $\mathbf{A}$
- $\mathbf{S}$  is *diagonal* (with decreasing coefficients) and of size  $(K+1) \times (K+1)$
- $\mathbf{V}$  is *unitary* and of size  $(K+1) \times (K+1)$

## Total least-squares

The estimation of the innovations are then obtained as follows

- $t_k$ : by finding the **roots** of the polynomial  $H(z)$
- $x_k$ : by least-square minimization of

$$\begin{bmatrix} \varphi(T-t_1) & \varphi(T-t_2) & \cdots & \varphi(T-t_K) \\ \varphi(2T-t_1) & \varphi(2T-t_2) & \cdots & \varphi(2T-t_K) \\ \vdots & \vdots & & \vdots \\ \varphi(NT-t_1) & \varphi(NT-t_2) & \cdots & \varphi(NT-t_K) \end{bmatrix} \begin{bmatrix} x_1 \\ x_2 \\ \vdots \\ x_K \end{bmatrix} = \begin{bmatrix} y_1 \\ y_2 \\ \vdots \\ y_N \end{bmatrix}$$

NOTE:

- Related to Pisarenko method
- Not robust with respect to noise  $\leadsto$  need for extra denoising

## Cadzow iterated denoising

Without noise, the annihilation property  $\mathbf{A}\mathbf{H} = 0$  still holds if  $\text{length}(\mathbf{H}) = L + 1$  is *larger* than  $K + 1$ . We have the properties

- $\mathbf{A}$  is still of **rank  $K$**
- $\mathbf{A}$  is a **Tœplitz matrix**
- conversely, if  $\mathbf{A}$  is Tœplitz and has rank  $K$ , then  $y_n$  are the **samples of an FRI signal**

### Rank $K$ "projection" algorithm

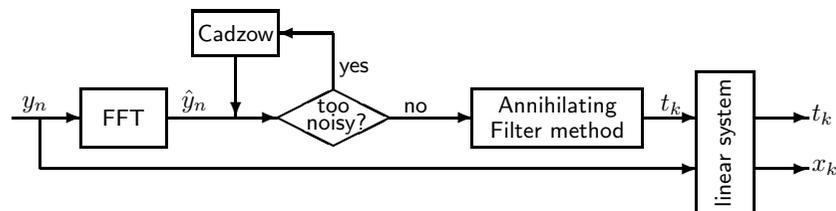
- 1 Perform the SVD of  $\mathbf{A}$ :  $\mathbf{A} = \mathbf{U}\mathbf{S}\mathbf{V}^T$
- 2 Set to zero the  $L - K + 1$  smallest diagonal elements of  $\mathbf{S} \rightsquigarrow \mathbf{S}'$
- 3 build  $\mathbf{A}' = \mathbf{U}\mathbf{S}'\mathbf{V}^T$
- 4 find the Tœplitz matrix that is closest to  $\mathbf{A}'$  and goto step 1

## Cadzow iterated denoising

### Essential details

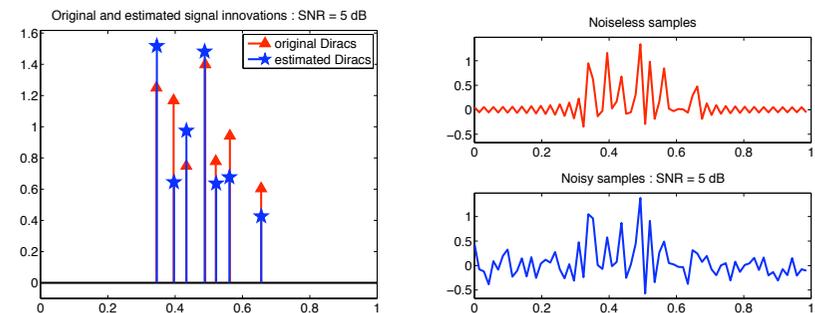
- Iterations of the projection algorithm are performed *until the matrix  $\mathbf{A}$  is of "effective" rank  $K$*
- $L$  is chosen *maximal*, i.e.,  $L = M$

Schematical view of the whole retrieval algorithm



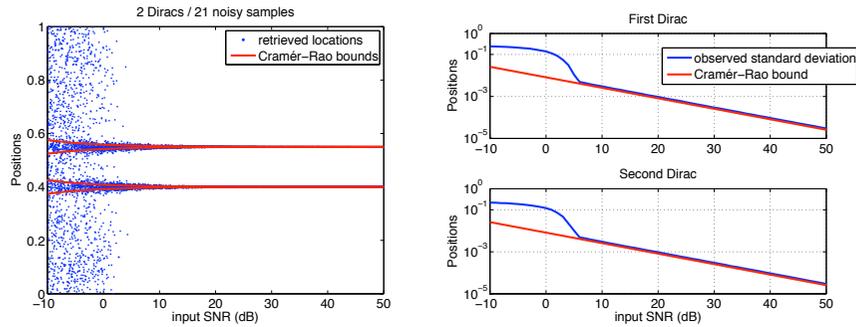
<sup>1</sup>T. Blu et al., "Sparse Sampling of Signal Innovations," *IEEE Signal Processing Magazine*, vol. 25, pp. 31–40, March 2008.

## Examples



Retrieval of an FRI signal with 7 Diracs (left) from 71 noisy (SNR = 5 dB) samples (right).

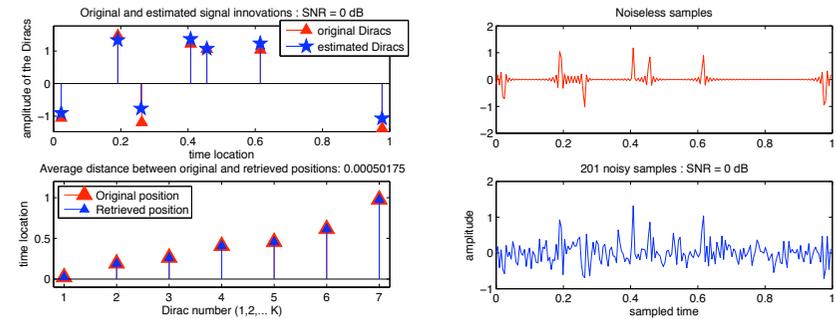
## Simulations: Quasi-optimality



Retrieval of the locations of a FRI signal. Left: scatterplot of the locations; right: standard deviation (averages over 10000 realizations) compared to Cramér-Rao lower bounds.

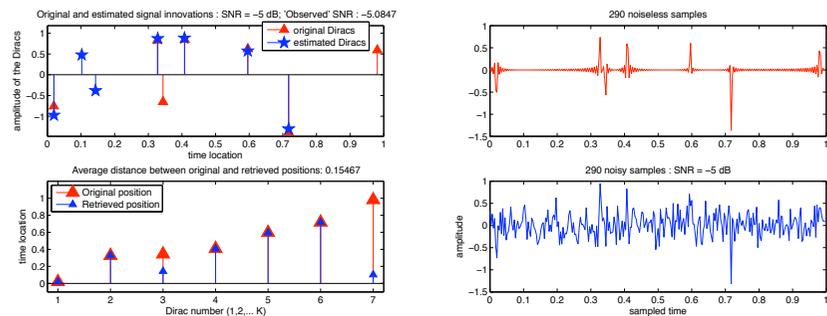
Quasi-optimality of the algorithm.

## Simulations: Robustness



201 samples of an FRI signal in 0 dB noise. Right: noiseless and noisy signal. Left: retrieved locations and amplitudes.

## Simulations: Robustness



290 samples of an FRI signal in -5 dB noise. Right: noiseless and noisy signal. Left: retrieved locations and amplitudes.

In high noise levels, the algorithm is still able to find *accurately* a substantial proportion of Diracs

## Optical Coherence Tomography: Principle

Detection of coherent backscattered waves from an object by making *interferences* with a *low-coherence* reference wave. Measurement performed with a standard Michelson interferometer.

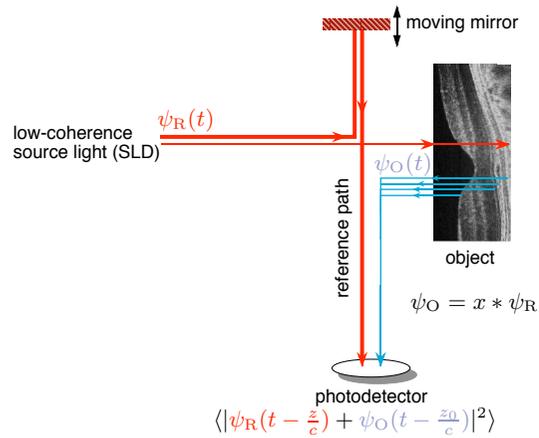
Axial (depth) resolution:  $\propto$  *coherence length* of the reference wave;  
Transversal resolution: width of the optical beam.

NOTE: *Very high sensitivity* (low SNR), noninvasive, low-depth penetration  
 $\leadsto$  biomedical applications (ophthalmology, dentistry, skin).  
Axial resolution<sup>2</sup>:  $10 \rightarrow 20 \mu\text{m}$ . Better resolution  $\rightarrow$  better diagnoses.

OCT is a ranging application!

<sup>2</sup>with SuperLuminescent Diodes: low cost, compact, easy to use.

## OCT: Experimental Setup



NOTE:  $z, z_0$  are the optical path lengths of the reference and the object wave.

## OCT: Mathematical setting

Measured intensity:

$$I_{\text{photo}}(z_0 - z) = \langle |\psi_R(t - \frac{z}{c}) + \psi_O(t - \frac{z_0}{c})|^2 \rangle$$

$$= \text{const} + \underbrace{2\Re\{(x * \varphi)(\frac{z-z_0}{c})\}}_{\text{OCT signal}}$$

↑  
variable (moving mirror)

$\varphi(t)$  is the temporal *coherence function* of the reference wave:

$$\varphi(t' - t) = \langle \psi_R(t'), \psi_R(t) \rangle$$

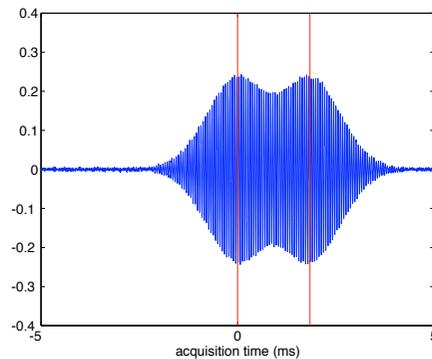
Typically,  $\varphi(t) \propto e^{-t^2/(2\sigma^2)} + 2i\pi\nu_0 t$  and  $x(t)$  is a stream of Diracs characterizing the depth of the interfaces, and the refractive index jumps.

An FRI interpolation problem

Retrieve  $x(t)$  from the uniform samples of the OCT signal.

## OCT: Resolution

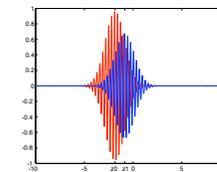
Resolution limit of OCT (two interfaces):  $L_c = c \times \text{FWHM of } A(t)$



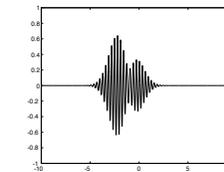
NOTE: Because the light travels twice (forward then backward) in the object, the actual *physical resolution* is  $L_c/2$ . Moreover, a larger value of refraction index inside the object further divides the resolution limit.

## OCT: Example of Processing

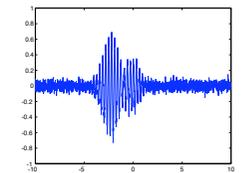
Separated Gaussians  
located at  $z_0$  and  $z_1$



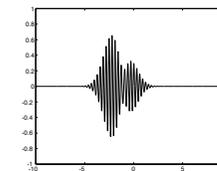
their sum



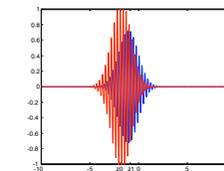
+ noise



resynthesized signal

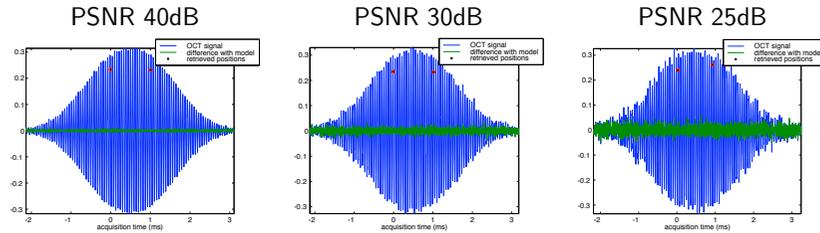


retrieved Gaussians



## OCT: Simulation example

Simulation examples: two interfaces distant by  $7\mu\text{m}$  (1ms below)



## OCT: Real Data Processing

SLD source of central wavelength  $0.814\mu\text{m}$  and coherence length  $25\mu\text{m}$ .  
 $\leadsto$  OCT resolution of  $12.5\mu\text{m}$ .

Depth scan of a  $4\mu\text{m}$  thick pellicle beamsplitter of an optical<sup>3</sup> depth of  $6.6\mu\text{m}$   $\leadsto$  approximately *half* the OCT resolution.

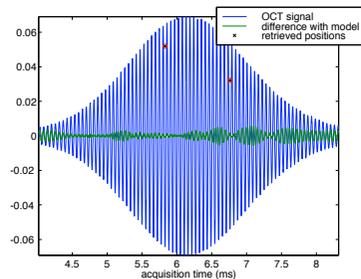
Calibration part:

- Depth scan of 1 interface  $\leadsto$  effective coherence function;
- High-coherence interferometer  $\leadsto$  accurate position of the moving mirror.

<sup>3</sup>refractive index 1.65.

## OCT: Real Data Processing

Example of superresolution: data-model PSNR=31dB



The two retrieved interfaces are distant by 17 interference fringes  
 $\leadsto 17 \times 0.814/2 = 6.9\mu\text{m}$ .

Presentation of a generic framework for interpolating samples under sparsity assumptions

- Super-resolution applications with noise-robust behaviour
- Unique solution as soon as  $2K$  measurements for  $2K$  unknowns
- Patents on the Dirichlet kernel transferred to Qualcomm

Papers available at <http://www.ee.cuhk.edu.hk/~tblu/>